

SPARSITY-ASSISTED SIGNAL SMOOTHING (REVISITED)

Ivan Selesnick

Electrical and Computer Engineering
Tandon School of Engineering, New York University
Brooklyn, New York, USA

ABSTRACT

This paper proposes an improved formulation of sparsity-assisted signal smoothing (SASS). The purpose of SASS is to filter/denoise a signal that has jump discontinuities in its derivative (of some designated order) but is otherwise smooth. SASS unifies conventional low-pass filtering and total variation denoising. The SASS algorithm depends on the formulation, in terms of banded Toeplitz matrices, of a zero-phase recursive discrete-time filter as applied to finite-length data. The improved formulation presented in this paper avoids the unwanted end-point transient artifacts which sometimes occur in the original version. For illustration, SASS is applied to ECG signal denoising.

Index Terms— low-pass filter, total variation, sparse signal, denoising, electrocardiogram.

1. INTRODUCTION

Numerous signals can be modeled as the sum of (1) a low-frequency signal and (2) a signal with a sparse K -order derivative. For example, an electrocardiogram (ECG) time-series can be modeled this way. A signal of this kind has jump discontinuities in its derivative (of order $K-1$) but is otherwise smooth. For the purpose of suppressing additive white Gaussian noise, conventional linear time-invariant (LTI) filters are not suitable for such a signal; LTI filtering tends to over smooth discontinuities (e.g., ‘corners’ of a signal). Similarly, (generalized) total variation (TV) denoising [29], which is intended for the denoising of piecewise constant (polynomial) signals, is also not suitable for such a signal; TV denoising tends to introduce staircase artifacts.

Sparsity-assisted signal smoothing (SASS) [31] was developed for the purpose of filtering a signal which has discontinuities in its derivative (of some designated order) but is otherwise smooth. SASS combines and unifies conventional LTI low-pass filtering and (generalized) TV denoising. Hence, SASS is useful for a wider class of signals than either LTI low-pass filtering or TV denoising is alone. The SASS algorithm formulates the denoising problem as a sparse deconvolution problem, and in turn, as an optimization problem comprising a data fidelity term and a sparse regularization term. The SASS problem formulation is expressed in terms of banded Toeplitz matrices. Furthermore, the computationally efficient implementation of SASS relies on fast solvers for banded systems of linear equations.

In this paper, we introduce an improved version of SASS.¹ Specifically, we improve the formulation, in terms of banded

Toeplitz matrices, of a class of recursive discrete-time filters as applied to finite-length data [31, 34]. This formulation is central to SASS because it allows linear low-pass filtering and nonlinear sparsity-based TV denoising to be combined in a single cost function to be minimized. However, the original formulation [31] gives rise to unwanted transient artifacts at the start and end of finite-length data. Avoiding those artifacts requires ad-hoc preprocessing of the input data which limits the applicability of SASS, especially for the filtering of short input data. The new matrix formulation presented in Sec. 2 below does not give rise to transient artifacts, hence no ad-hoc preprocessing is needed and SASS can be effectively applied to both short and long finite-length data.

1.1. Relation to Prior Work

Several prior works have studied the signal model considered here, i.e., a signal comprising the sum of low-frequency signal and a sparse-derivative signal [11, 16, 26, 32, 33, 34]. The most closely related relevant work is by Gholami and Hosseini [16] who combine Tikhonov (quadratic) regularization and TV denoising. In contrast to [16], SASS is formulated explicitly in terms of an LTI low-pass filter to which it reduces as a special case, and hence can be understood in terms of its frequency response; whereas, the method of [16] is formulated in terms of Tikhonov regularization. In addition, SASS is formulated to allow a higher-order sparse derivative and exploits a factorization (see (30) below) without which the estimated sparse-derivative signal component tends to be unbounded in the higher-order case, which hinders the usability of the result and impedes numerical stability of optimization algorithms. We note that Ref. [16] considers also the problems of deconvolution and compressed sensing, which are not considered here.

As SASS can be considered an extension of TV denoising, we note that several extensions of TV denoising have been proposed [3, 21, 23, 24]. In contrast to these methods, SASS can also be considered an extension of LTI filtering. SASS unifies TV denoising and LTI filtering, and hence conforms to and builds upon elementary signal processing.

Wavelet-based denoising is suitable for the type of piecewise-smooth signal considered here. But simple wavelet-domain denoising leads to artifacts; hence, wavelet-based signal models have been developed to explicitly account for singularities (i.e., discontinuities in the derivative of a signal), such as: hidden Markov tree [9], singularity detection [20, 22], wavelet footprints [12, 35], TV-wavelet [13, 14], and singularity approximation [4, 5]. Although SASS is less general than wavelet-based methods (it does not have a multiscale property), it is much simpler than wavelet-based methods because it does not involve wavelet-domain singularity modeling. SASS preserves sparse singularities in an otherwise smooth signal without inducing wavelet-like artifacts.

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¹Software is available online at <http://eeweb.poly.edu/iselesni/sass/>

2. FILTERS AS MATRICES

Given finite-length sequences p_n and q_n , we define banded Toeplitz matrices \mathbf{P} and \mathbf{Q} to have the form

$$\mathbf{P} = \begin{bmatrix} p_2 & p_1 & p_0 & & & \\ & p_2 & p_1 & p_0 & & \\ & & \ddots & & \ddots & \\ & & & p_2 & p_1 & p_0 \end{bmatrix} \quad (1)$$

$$\mathbf{Q} = \begin{bmatrix} q_2 & q_1 & q_0 & & & \\ & q_2 & q_1 & q_0 & & \\ & & \ddots & & \ddots & \\ & & & q_2 & q_1 & q_0 \end{bmatrix}. \quad (2)$$

By the relation between Toeplitz matrices and convolution, we have

$$[\mathbf{P}\mathbf{x}]_n = (p * x)(n) \quad (3)$$

where \mathbf{x} is vector containing values $x(n)$ and \mathbf{P} is appropriately indexed. Hence, the matrix \mathbf{P} corresponds to an LTI system with transfer function

$$P(z) = \sum_n p_n z^{-n} \quad (4)$$

and frequency response $P(e^{j\omega})$. The matrix \mathbf{Q} corresponds likewise to an LTI system.

Consider the cost function

$$J(\mathbf{x}) = \|\mathbf{Q}(\mathbf{y} - \mathbf{x})\|_2^2 + \alpha \|\mathbf{P}\mathbf{x}\|_2^2 \quad (5)$$

with $\alpha > 0$. The function J is minimized by

$$\mathbf{x} = (\mathbf{Q}^T\mathbf{Q} + \alpha\mathbf{P}^T\mathbf{P})^{-1}\mathbf{Q}^T\mathbf{Q}\mathbf{y} \quad (6)$$

which constitutes a linear filter with matrix

$$\mathbf{H} = (\mathbf{Q}^T\mathbf{Q} + \alpha\mathbf{P}^T\mathbf{P})^{-1}\mathbf{Q}^T\mathbf{Q}. \quad (7)$$

We define

$$\mathbf{A} := \mathbf{Q}^T\mathbf{Q} + \alpha\mathbf{P}^T\mathbf{P} \quad (8)$$

where we note that \mathbf{A} is *banded*. We thus write \mathbf{H} as

$$\mathbf{H} = \mathbf{A}^{-1}\mathbf{Q}^T\mathbf{Q}. \quad (9)$$

Note that \mathbf{H} is not banded, even though \mathbf{A} and \mathbf{Q} are. Fortunately, the efficient implementation of (6) requires only \mathbf{A} and \mathbf{Q} be banded.

The matrix \mathbf{H} is approximately Toeplitz; thus, it represents (approximately) an LTI system, the frequency response of which is

$$H(e^{j\omega}) = \frac{|Q(e^{j\omega})|^2}{|Q(e^{j\omega})|^2 + \alpha|P(e^{j\omega})|^2}. \quad (10)$$

Note that $H(e^{j\omega})$ is zero-phase (i.e., real-valued). The transfer function is given by

$$H(z) = \frac{Q(z)Q(1/z)}{Q(z)Q(1/z) + \alpha P(z)P(1/z)}. \quad (11)$$

Expression (6) implements a zero-phase recursive discrete-time filter for finite-length data. It can be considered a type of forward-backward filtering (e.g., `filtfilt` in Matlab or `scipy.signal.filtfilt` in Python). An advantage of (6) is that transient effects at the start and end of the finite-length signal

are intrinsically avoided. This is because each row of the convolution matrices \mathbf{P} and \mathbf{Q} in (1) and (2) contains a full impulse response (not truncated). (This is akin to the `valid` option in the Matlab `conv` function or the Python `numpy.convolve` function.) Therefore, using expression (6), it is not necessary to specify internal filter states or perform symmetric extensions, which are usual ways to avoid transient end-point artifacts in forward-backward filtering.

The implementation of (6) requires the solution of a system of linear equations. Fast memory-efficient solvers for banded systems can be used for this purpose [28, Sect 2.4].

2.1. High-pass Filter

If H is a zero-phase low-pass filter, then $G = I - H$ is a zero-phase high-pass filter with transfer function

$$G(z) = \frac{\alpha P(z)P(1/z)}{Q(z)Q(1/z) + \alpha P(z)P(1/z)}. \quad (12)$$

Using (8) and (9), the filter matrices for G are given by

$$\mathbf{G} = \mathbf{I} - \mathbf{H} \quad (13)$$

$$= \mathbf{I} - \mathbf{A}^{-1}\mathbf{Q}^T\mathbf{Q} \quad (14)$$

$$= \mathbf{A}^{-1}(\mathbf{A} - \mathbf{Q}^T\mathbf{Q}) \quad (15)$$

$$= \alpha\mathbf{A}^{-1}\mathbf{P}^T\mathbf{P} \quad (16)$$

where we used (8) to simplify (15).

2.2. Butterworth Low-pass Filter

Some classical filters have transfer functions of the form (11). From (11), note that

$$P(z_0) = 0 \implies H(z_0) = 1 \quad (17)$$

$$Q(z_0) = 0 \implies H(z_0) = 0. \quad (18)$$

In this paper, we set

$$P(z) = (1 - z^{-1})^d \quad (19)$$

$$Q(z) = (1 + z^{-1})^d \quad (20)$$

for a positive integer d , leading to $P(1) = 0$ and $Q(-1) = 0$, i.e., $H(1) = 1$ and $H(-1) = 0$. Hence, the frequency response of the filter H has unity gain at $\omega = 0$ and a null at $\omega = \pi$. Furthermore, the frequency response is flat at these two points (its first few derivatives are zero, depending on d).

With $P(z)$ and $Q(z)$ given by (19) and (20), the filter H in (11) is a discrete-time Butterworth filter [27]. The frequency response of H is given by

$$H(e^{j\omega}) = \frac{\cos^{2d}(\omega/2)}{\cos^{2d}(\omega/2) + \alpha \sin^{2d}(\omega/2)}. \quad (21)$$

We can set α so the frequency response has a designated cut-off frequency ω_c . Setting $H(e^{j\omega_c}) = 0.5$ and solving for α yields

$$\alpha = 1/\tan^{2d}(\omega_c/2). \quad (22)$$

The zero-phase Butterworth filter, implemented for finite-length signals using (6), exactly preserves polynomial input signals up to degree $2d - 1$ (with no transients at signal end-points). This is due to the flatness of $H(z)$ at $z = 1$. The Savitzky-Golay filter [30] also has this polynomial approximation property.

where \mathbf{x}_1 is a signal with sparse K -order derivative, i.e., $\mathbf{D}\mathbf{x}_1$ is sparse. Let us use $P(z)$ and $G(z)$ with parameter d with $K \leq d$. Then $\mathbf{P} = \mathbf{P}_1\mathbf{D}$ from (30), so we write (37) as

$$\hat{\mathbf{x}} = \mathbf{A}^{-1}\mathbf{Q}^T\mathbf{Q}\mathbf{y} + \alpha\mathbf{A}^{-1}\mathbf{P}^T\mathbf{P}_1\mathbf{D}\mathbf{x}_1. \quad (38)$$

Since $\mathbf{D}\mathbf{x}_1$ is sparse, we write the signal model as

$$\hat{\mathbf{x}} = \mathbf{A}^{-1}\mathbf{Q}^T\mathbf{Q}\mathbf{y} + \alpha\mathbf{A}^{-1}\mathbf{P}^T\mathbf{P}_1\mathbf{u} \quad (39)$$

where \mathbf{u} is sparse (and is to be determined/optimized).

Hence, a suitable cost function to determine \mathbf{u} is

$$J(\mathbf{u}) = \frac{1}{2}\|\mathbf{y} - \mathbf{A}^{-1}\mathbf{Q}^T\mathbf{Q}\mathbf{y} - \alpha\mathbf{A}^{-1}\mathbf{P}^T\mathbf{P}_1\mathbf{u}\|_2^2 + \lambda\|\mathbf{u}\|_1$$

where the ℓ_1 norm is used to induce sparsity of \mathbf{u} . The quadratic data fidelity term corresponds to the additive white Gaussian noise assumption. Using (16), we have

$$\mathbf{y} - \mathbf{A}^{-1}\mathbf{Q}^T\mathbf{Q}\mathbf{y} = \alpha\mathbf{A}^{-1}\mathbf{P}^T\mathbf{P}\mathbf{y}, \quad (40)$$

i.e.,

$$y - \text{LPF}\{y\} = \text{HPF}\{y\}, \quad (41)$$

so the cost function to be minimized can be written as

$$J(\mathbf{u}) = \frac{\alpha^2}{2}\|\mathbf{A}^{-1}\mathbf{P}^T(\mathbf{P}\mathbf{y} - \mathbf{P}_1\mathbf{u})\|_2^2 + \lambda\|\mathbf{u}\|_1 \quad (42)$$

To clarify/summarize the matrix sizes: If $\mathbf{y} \in \mathbb{R}^N$, then

$$\mathbf{u} \in \mathbb{R}^{N-K}, \quad \mathbf{P}_1 \in \mathbb{R}^{(N-d) \times (N-K)}, \quad (43)$$

$$\mathbf{A} \in \mathbb{R}^{N \times N}, \quad \mathbf{P} \in \mathbb{R}^{(N-d) \times N}. \quad (44)$$

The minimization of the cost function J in (42) is the standard ℓ_1 -norm sparse least squares problem arising in basis pursuit denoising, compressed sensing [6], etc. It can be solved by the iterative shrinkage/thresholding algorithm (ISTA) [10, 15] (an instance of forward-backward splitting [7, 8]), accelerated variants of ISTA (FISTA [2], FASTA [18], etc.), alternating direction method of multipliers (ADMM) [1, 17], iterative reweighted least-squares (IRLS) [19], etc. Therefore, we omit details about how to perform the minimization of the cost function J . We note only that all matrices \mathbf{A} , \mathbf{P} , and \mathbf{P}_1 are banded; thus, algorithms can be implemented with high computational efficiency, as described in [31].

A key point in the above formulation is that, even though we model $\mathbf{D}\mathbf{x}_1$ as sparse, the matrix \mathbf{D} does not appear in the ℓ_1 -norm penalty term of the cost function (42). Instead of penalizing $\mathbf{D}\mathbf{x}_1$, we penalize \mathbf{u} . This simplifies the problem and its algorithmic solution. This simplification is possible because \mathbf{D} is a factor of \mathbf{P} as related in (30), i.e., $D(z)$ is a factor of $P(z)$.

4. EXAMPLE

This example uses sparsity-assisted signal smoothing (SASS) to denoise the noisy ECG signal shown in Fig. 2(a). We simulate the ECG signal using ECGSYN [25] and add white Gaussian noise. The ECG signal exhibits abrupt changes in its slope. So, it seems reasonable to model the ECG signal as a low-frequency signal plus a signal with a sparse second-order derivative (i.e., with jump discontinuities in its first-order derivative). Hence, we set $K = 2$ in SASS.

For SASS, the low-pass filter H must also be specified. We set $d = 2$ which satisfies $K \leq d$ as required. We set the cut-off frequency to $\omega_c = 0.06\pi$ (i.e., $f_c = 0.03$ in normalized frequency

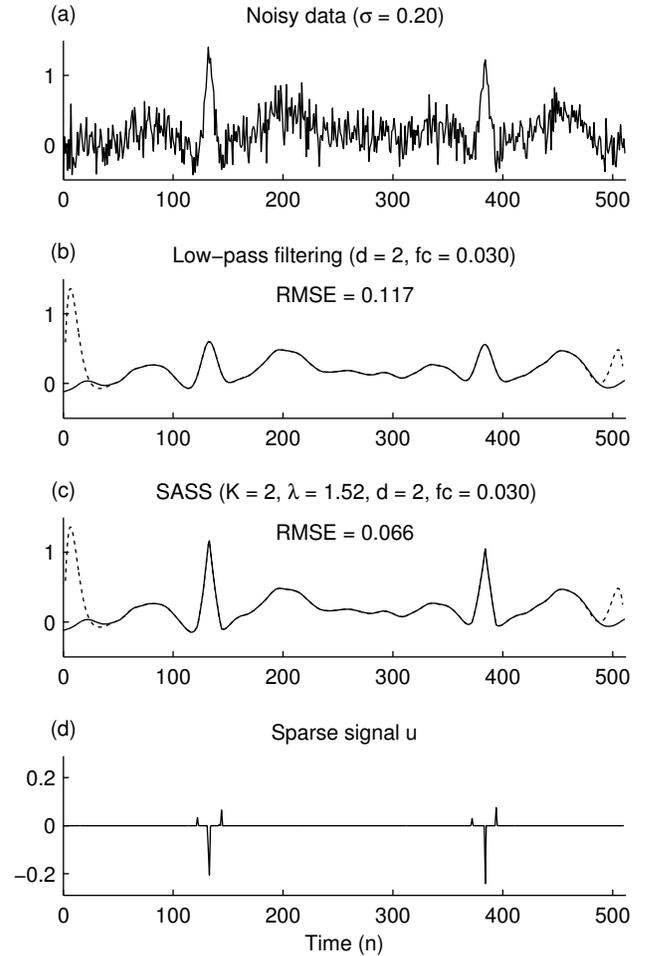


Fig. 2: Denoising of a simulated ECG signal. (The dashed line is the old formulation which has end-point transient artifacts.)

units). This leads to $\alpha = 12524.52$ using (22). The parameters d and α define the zero-phase Butterworth filters H and G , i.e., the matrices \mathbf{P} , \mathbf{Q} , and \mathbf{A} . As Fig. 2(b) shows, this low-pass filter by itself substantially suppresses the noise and smooths the signal. But it severely distorts the sharp peaks of the ECG waveform.

The output of SASS, shown in Fig. 2(c), accurately preserves the sharp peaks of the ECG waveform. Indeed, the first-order derivative of the SASS-denoised signal has jump discontinuities in several places. The sparse signal u , computed as part of the method, is shown in Fig. 2(d). It is the non-zero values of u that produce the jump discontinuities of the first-order derivative of the denoised signal. The denoised signal is given by (39) where u is obtained by minimizing the cost function (42). We have set the value of the parameter λ using the method suggested in [31]. As Fig. 2 shows, the proposed reformulation of SASS avoids the occurrence of unwanted end-point transient artifacts.

5. CONCLUSION

Sparsity-assisted signal smoothing (SASS) depends on a banded matrix formulation of recursive filtering of finite-length input signals. This paper presents a formulation that avoids the unwanted transient artifacts at signal end-points in the original formulation [31, 34].

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